### Formulation and Evaluation of Fast Dissolving Film of Lisinopril

### Siddhesh Gawari\*, S. R. Ghodake

Loknete Shri Dada patil pharate College of pharmacy

#### ABSTRACT

"An ultra-thin film containing an active ingredient that dissolves or disintegrates in the saliva at aremarkably fast rate, within few seconds without the aid of water or chewing," is the definition of fast-dissolving oral film (FDOF). The most up-to-date oral solid dosage form is fast-dissolving oral films (FDOFs), which provide more comfort and flexibility. It improves the absorption of active pharmaceutical ingredients (APIs) by dissolving them in saliva and allowing them to be swallowed without chewing or water. The oral mucosa is four to a thousand times more permeable than the epidermis, allowing for rapid drug absorption and rapid bioavailability. Formulated drug- opening foams (FDOFs) are made from hydrophilic polymers that dissolve rapidly in the mouth and release the medication into the bloodstream via the buccal mucosa. [1] A fast-dissolving drug delivery method is developed to enhance bioavailability of drugs with modest dosages and significant first-pass metabolism.

Keywords: Fast Dissolving Film, Lisinopril, FDOF, APIs

#### **INTRODUCTION**

1.2 Oral Dissolving Film Theory:

In this setup, a thin film is present. Sublingual administration improves bioavailability because the drug dissolves faster and bypasses first-pass metabolism. Because SA is more easily absorbed, it breaks down and dissolves rapidly in the mouth. The following are the three main types of oral films: 1.Films have a rapid dissolving or releasing time (when held to the mouth).

2.Mucoadhesive films that dissolve (for use in the buccal or gingival area). The third option is buccal mucosa-adhering sustained-release films. [3]

### **1.3** Mechanism of oral mouth dissolving film theory:



**Relevant conflicts of interest/financial disclosures**: The authors declare that the research was conducted in the absence of any commercial or financial relationships that could be construed as a potential conflict of interest.



Figure 2: Mouth-dissolving film

## 1.4 Need for fast-dissolving drug delivery systems:[4]

Patients with dysphasia may find it easier to take their medication as prescribed when it dissolves quickly. If a medicine is subject to patent protection, the marketing department will find that FDDS is a useful tool for managing the medical life cycle.

#### **METHODS**

#### 1 Solvent casting method [81]

Fast dissolving films were prepared by solvent casting method as per the composition shown in table 1.In this method, the required quantity of water soluble polymer Sodium carboxymethyl cellulose was dissolved in distilled water in a beaker (covered with aluminium foil) with continuous stirring on magnetic stirrer to make required percentage of polymer solution and then the weighed quantity of ingredients like lisinopril as drug , glycerol as plasticizer, and menthol a flavor, Saccharin sodium as Sweetening agent was dissolved in distilled water in another beaker and then this mixture was added to the polymer solution. After continuous stirring for 2 hours the solution was left undisturbed for 12 - 16 hours to remove all the air bubbles. This polymeric – drug solution was then poured on to the moulds, allowed to air dry , packed in aluminum foil and then stored in desiccators until use.



#### Advantages

•Film has a fine gloss and is devoid of flaws like die lines, and it has superior uniformity of thickness and clarity to extrusion. •The recommended finished film thickness is typically 12-100 m; however different

thicknesses are available to fulfill API loading and dissolving needs. The film has better physical qualities and is more flexible.

#### **Disadvantages:**

1. The polymer needs to be soluble in water or a volatile solvent.

2.It is ideal to generate a stable solution with a reasonable minimum solid content and viscosity.

3.It must be feasible to create a homogeneous film and be released from the casting support.

#### 6.2.2 Experimental Design [82]

Box–Behnken design was employed to studythe effect of each independent variable on dependent variables Disintegration time (sec), Drug content (%) and Drug release (%) Lisinopril film formulation were prepared by solvent casting method. The Lisinopril film were optimized by using Box-Behnken Experimental Design (3 Factor, 2 Level, and DesignExpert Version 13). The independent variables selected were Sodium carboxymethyl cellulose(mg) (X1), Sodium starch glycolate(mg) (X2) and Glycerol(ml) (X3) with their low and high levels for preparing 13 run of formulations and dependent variable selected were Disintegration time(sec) , (wetting time (sec) and Drug release (%). Finally optimized was selected for further characterization.

Table 14. DOE suggested and experimental batches							
Formul ation	Lisinopril (mg)	Sodium carboxymethyl	Sodium starch	Glycerol (ml)	Sacchari n sodium	Menthol (ml)	Distilled water(ml)
code	(	cellulose (mg)	glycolate(mg)	(1111)	(mg)	(111)	(iiii)
L1	158.96	450	10	0.5	10	0. S	O. S
L2	158.96	450	11	0.75	10	0. S	0. S
L3	158.96	650	10	0.75	10	Q. S	Q. S
L4	158.96	650	12	0.75	10	Q. S	Q. S
L5	158.96	250	11	1	10	Q. S	Q. S
L6	158.96	250	11	0.5	10	Q. S	Q. S
L7	158.96	250	10	0.75	10	Q. S	Q. S
L8	158.96	450	10	1	10	Q. S	Q. S
L9	158.96	650	11	1	10	Q. S	Q. S
L10	158.96	450	12	1	10	Q. S	Q. S
L11	158.96	250	12	0.75	10	Q. S	Q. S
L12	158.96	450	12	0.5	10	Q. S	Q. S
L13	158.96	650	11	0.5	10	Q. S	Q. S

Table 14: DOE suggested and experimental batches

#### **Calculation for Petri Dish**

Diameter of Petri dish = 9cm Area of circle =  $= 3.14 \times 4.5 \times 4.5$ 

=63.585 cm2

Area of Single patch =  $L \times W$  Area of Single patch =  $2 \times 2$ 

= 4 cm 2

So, Total no of films = 63.585 / 4 =15.89

Total amount of drug requires = i.e. (Total no of films  $\times$  Dose of drug) = 15.896 $\times$ 10 Total amount of drug require =158.96 mg





Independent Variable	Low (-1)	High (+)
Sodium carboxymethyl cellulose(mg)	250	450
Sodium starch glycolate(mg)	10	12
Glycerol(ml)	0.5	1
Dependent Variable	Constraint	
Disintegration time(sec)	Maximize	
Drug content (%)	Maximize	
Drug release (%)	Maximize	

#### Table 15: List of independent variable and dependent variable on box Behnken design

#### **RESULT AND DISCUSSION**

#### 7.1.1 Identification of drug

#### 7.1 PREFORMULATION STUDY

#### 1.1.1.1 Appearance



**7.1.1.2 Active pharmaceutical ingredient:** Lisinopril

#### 7.1.2 Melting point

The capillary tube method was used to determine the melting point. The melting point of Lisinopril was found to be 164 and recorded melting point of Lisinopril 162-165 °C.

# Table 16: Observation of melting pointDrug nameObserved valueReported valueLisinopril164162-165



Figure 10: Melting point of Lisinopril



#### 7.1.3 Solubility study of lisinopril

The solubility study of lisinopril across various mediums reveals that methanol provides the highest solubility at 48.16 mg/mL, making it the most

effective solvent for dissolving lisinopril. Ethanol (30.14 mg/mL) and distilled water (29.14 mg/mL) also demonstrate good solubility, suggesting they are suitable alternatives for formulation purposes.

Tuble 177 Bolubility in unter ent intertain		
Solubility(mg/ml)		
29.14		
48.16		
30.14		
28.46		
26.54		
21.46		

Table 17: Solubility	in different Medium
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Figure 11: Solubility in different Medium

7.1.2 Spectrophotometric characterization of 7.1.2.1 Detection of Absorption Maxima ( $\lambda$  max) Lisinopril in UV Spectroscopy

Table 18: Observation of $\lambda$ max			
Drug name	Observed value(nm)	Reported value(nm)	
Cilnidipine	210	210-220	

#### 7.1.2.2 Calibration curve

Tuble 177 Cullbrution cullye in Distinct water		
Concentration (µg/ml)	Absorbance	
0	0	
2	0.015	
4	0.021	
6	0.035	
8	0.052	
10	0.062	
12	0.071	

#### Table 19: Calibration curve in Distilled water





Figure 12: Calibration curve in Distilled water

Equation	y = 0.006x + 0.0004
Correlation coefficient	0.9909

#### 7.1.2.2.2 Calibration curve in Methanol

Table 20: Calibration curve in Methanol		
Concentration (µg/ml)	Absorbance	
0	0	
2	0.125	
4	0.235	

0.354

0.487

0.587

0.747

6

8

10

12



**Figure 13: Calibration curve in Methanol** 

Equation	y = 0.061x - 0.004
Correlation coefficient	0.9979

#### 7.1.2.2.3 Calibration curve in Ethanol

Table 21: Calibration curve in Ethanol		
Absorbance		
0		
0.125		
0.185		
0.350		
0.427		
0.589		
0.647		



#### Figure 14: Calibration curve in ethanol

Equation	y = 0.0556x - 0.0015
Correlation coefficient	0.9895

### 7.1.2.2.4 Calibration curve in Phosphate buffer pH 6.8

#### Table 22: Calibration curve in Phosphate buffer pH 6.8

Concentration (µg/ml)	Absorbance
0	0
2	0.012
4	0.125
6	0.251
8	0.416
10	0.520
12	0.640





Figure 15: Calibration curve in Phosphate buffer pH 6.8

Equation	y = 0.0576x - 0.0652
Correlation coefficient	0.9767

7.1.2.2.5 Calibration curve in Phosphate buffer pH 7.4

Concentration (µg/ml)	Absorbance
0	0
2	0.125
4	0.198
6	0.224
8	0.314
10	0.456
12	0.489





Equation	y = 0.0401x + 0.0175
Correlation coefficient	0.9745

#### 7.1.2.2.6 Calibration curve in Acidic buffer pH 1.2

Concentration (µg/ml)	Absorbance
0	0
2	0.122
4	0.132
6	0.169
8	0.241
10	0.3997
12	0.487



Figure 17: Calibration curve in Acidic buffer pH 1.2

#### 7.2 Post Formulation Study

#### 7.2.1 Transparency

Physical appearance of the formulations. The clear transparency indicates that there are no visible

particles or impurities present in any of the formulations. Additionally, the optimization of batch L8 suggests that it meets the desired criteria for clarity and uniformity, making it the preferred choice for further development or use in applications requiring clear formulations.

······································	
Formulation code	Transparency
L1	Clear
L2	Clear
L3	Clear
L4	Clear
L5	Clear
L6	Clear
L7	Clear
L8	Clear
L9	Clear
L10	Clear



L11	Clear
L12	Clear
L13	Clear

#### 7.2.2Weight Variation

The optimized batch (L8) of the fast dissolving film formulation exhibited a weight variation of  $46.4 \pm 0.24$ . This result indicates a consistent weight among different units of the film, ensuring uniformity in dosage. A low variation in weight is crucial for

maintaining the quality and efficacy of the pharmaceutical product. Therefore, batch L8 meets the desired standards for weight uniformity in the formulation.

#### 26: Weight Variation L1to L13

Formulation code	Weight Variation (mg)
L1	54.6±0.01
L2	62.56±0.02
L3	58.46±0.03
L4	89.1±0.01
L5	79.9±005
L6	87.3±0.12
L7	91.46±0.03
L8	46.4±0.24
L9	79±0.03
L10	47±0.15
L11	49±0.02
L12	36.56±0.06
L13	62.3±0.005

#### 7.2.3 Moisture content

#### 27: Moisture content L1to L13

Moisture content data, formulation L8 emerges as the optimized choice due to its comparatively low moisture content of  $2.7\% \pm 0.546$ .

Formulation code	Moisture content (%)
L1	$4\pm0.879$
L2	$5\pm0.546$
L3	$4.5 \pm 0.442$
L4	6± 0.534
L5	$5.2\pm0.945$
L6	$6.2 \pm 0.764$
L7	7.1±0.345
L8	$2.7 \pm 0.546$
L9	$5.4 \pm 0.142$
L10	$4.6 \pm 0.503$
L11	3±0.511
L12	2.9±0.234
L13	3.5±0.141

#### 7.2.4 Thickness (mm)

The optimized batch (L8) of the fast dissolving film formulation exhibited a thickness of  $0.14 \pm 0.010$  mm.

#### 28: Thickness (mm) L1to L13

Formulation code	Thickness(mm)
L1	$0.11 \pm 0.0.1$
L2	$0.13 \pm 0.0.2$
L3	$0.10\pm0.01$
L4	$0.16\pm0.005$
L5	$0.15\pm0.03$
L6	$0.14 \pm 0.04$
L7	$0.9\pm0.005$
L8	$0.14\pm0.010$
L9	$0.16\pm0.005$
L10	$0.11 \pm 0.05$
L11	0.9±0.01
L12	0.17±0.02
L13	0.15±0.04

#### 7.2.5 Folding endurance study

29: Folding endurance L1to L13

The optimized batch (18) of the fast dissolving film formulation demonstrated excellent folding endurance, with a value exceeding 300.

Formulation code	Folding endurance
L1	> 300
L2	> 300
L3	> 300
L4	150
L5	209
L6	> 300
L7	124
L8	> 300
L9	130
L10	> 300
L11	> 300
L12	> 300
L13	> 300

#### 7.2.6 Surface pH

The optimized fast dissolving film formulation (18) exhibited a pH of 6.1.

Table 30: PH of L1to L13				
Formulation code	ph			
L1	6.3±0.002			
L2	6.40. ±003			
L3	6.13±0.06			
L4	6.7±0.07			
L5	6.5±0.07			
L6	6.83±0.06			
L7	7.13±0.05			
L8	6.1±0.06			
L9	6.94±0.03			
L10	6.67±0.04			



L11	6.70±0.06
L12	$6.56 \pm 0.05$
L13	6.59±0.012

7.2.7 Drug Content (%)

Formulation L8 exhibits the highest drug content among the tested formulations, with a percentage of 96.48%.

Drug Content (%)				
87.89				
90.16				
89.98				
93				
86.65				
73.56				
89.13				
96.48				
88.36				
94.56				
79				
78.46				
88.49				

#### Table 31: Drug Content (%) of L1to L13

ANOVA for Linear model Response 2: Drug content

Source	Sum of	df	Mean	F-	р-	
	Squares		Square	value	value	
Model	343.74	3	114.58	5.62	0.0189	significant
A-Sodium carboxymethyl	123.95	1	123.95	6.08	0.0358	
B-Sodium starch glycolate	42 60	1	42 60	2.09	0 1823	
C-glycerol	177.19	1	177.19	8.69	0.0163	
Residual	183.52	9	20.39			
Cor Total	527.26	12				

#### Factor coding is coded. Factor Coding: Actual

Drug content (%) Design Points

96.48

7356

X1 = A X2 = B

Actual Factor C = 0.75







#### Figure 20: 3D Surface plot

#### 7.2.8 Tensile strength (N/mm<sup>2</sup>)

The tensile strength of formulation L8 is determined to be  $3.4 \pm 0.14$  N/mm<sup>2</sup>, positioning it as the optimized

batch among the formulations tested. This suggests that formulation L8 possesses favorable mechanical characteristics, which are crucial for the integrity and performance of the product.

Formulation code	Tensile strength((N/mm <sup>2</sup> ))
L1	$5.3 \pm 0.01$
L2	$6.9\pm0.02$
L3	$6.8 \pm 0.04$
L4	$4.3\pm0.02$
L5	$3.9 \pm 0.03$
L6	$9.5 \pm 0.02$
L7	4.1 ± 0.23
L8	$3.4 \pm 0.14$

 Table 32: Tensile strength (N/mm²) of L1to L13

L9	$4.8 \pm 0.05$
L10	$7.6\pm0.04$
L11	$5.4 \pm 0.03$
L12	$6.7 \pm 0.13$
L13	$7.4 \pm 0.5$

#### **7.2.9 Percentage elongation (%)**

Percentage elongation for various formulations ranges from 13.6% to 45.26%.

Table 55. I creentage clongation (70) of Lito Lis				
Formulation code	Percentage elongation (%)			
L1	$27.4 \pm 0.12$			
L2	$33.2 \pm 0.07$			
L3	$34.2\pm0.01$			
L4	$17.0 \pm 0.14$			
L5	$16.8 \pm 0.34$			
L6	$45.26\pm0.010$			
L7	$13.6 \pm 0.05$			
L8	$39.3 \pm 0.12$			
L9	$22.1 \pm 0.30$			
L10	$37.0 \pm 0.15$			
L11	$26.5 \pm 0.10$			
L12	$30.3 \pm 0.07$			
L13	$38.0 \pm 0.14$			

### Table 33: Percentage elongation (%) of L1to L13

#### 7.2.10. in Vitro Disintegration Time

The disintegration time for various formulations of fast-dissolving oral films (batch L8) ranges from 22 to 62 seconds.

Formulation code	Disintegration Time(sec)
L1	35
L2	38
L3	53
L4	62
L5	29
L6	28
L7	32
L8	22
L9	53
L10	27
L11	30
L12	43
L13	37

#### Table 34: Disintegration Time of L1to L13

## ANOVA for Linear model Response 1: disintegration time

Source	Sum of Squares	df	Mean Square	F- value	p- value	
Model	992.50	3	330.83	4.11	0.0431	significant
A-Sodium	924.50	1	924.50	11.48	0.0080	
carboxymethyl cellulose						



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<b>B-Sodium</b> starch	50.00	1	50.00	0.6211	0.4509	
glycolate						
C-glycerol	18.00	1	18.00	0.2236	0.6476	
Residual	724.58	9	80.51			
Cor Total	1717.08	2				

#### Factor coding is coded. Sum of squares is Type III - Partial



Figure 22: Predicted vs Actual plot



Figure 23: 3D Surface plot

#### 7.2.11 In Vitro drug release study

The in-vitro diffusion study for the L8 optimized batch shows exceptional performance, with an initial drug release of  $20.56\% \pm 0.04$  at 1 minute and reaching a near-complete release of  $98.99\% \pm 0.687$ at 10 minutes.

		Table 55.	Diug i cicase (	<i>n</i> <b>D</b> 1-D0		
Time (min)	L1	L2	L3	L4	L5	L6
0	0	0	0	0	0	0
1	23.56±0.01	19.46±0.03	15.46±0.03	20.46±0.03	$17.89 \pm 0.005$	17.89±0.05
2	35.56±0.02	32.56±0.06	30.12±0.01	30.44±0.05	29.45±0.156	28.79±0.01
3	45.63±0.123	44.78±0.05	41.35±0.156	43.56±0.06	38.89±0.05	35.44±0.02
4	52.64±0.05	50.16±0.04	50.66±0.04	53.49±0.08	49.89±0.063	49.76±0.05
5	62.49±0.03	64.64±0.346	58.79±0.04	61.44±0.07	57.89±0.741	53.66±0.06
6	69.25±0.01	69.77±0.254	63.55±0.632	73.89±0.05	68.79±0.523	69.88±0.05
7	73.44±0.06	74.56±0.03	71.46±0.542	77.46±0.04	74.56±0.03	79.98±.01
8	78.36±0.314	81.66±0.02	79.86±0.31	84.53±0.01	80.16±0.04	86.56±0.03
9	84.56±0.03	$88.66 \pm 0.467$	86.56±0.04	89.65±0.02	85.66±0.345	90.16±0.04
10	86±0.146	90.13±0.05	89.46±0.03	91±0.01	89.87±0.01	94.58±0.01

able 35: Drug	release of L1-L6
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All values expressed as mean  $\pm$  SD (n=3)

Table 36: Drug release of L7-L13

		_		8			
Time	L7	L8	L9	L10	L11	L12	L13
(min)							
0	0	0	0	0	0	0	0
1	16.56±0.0	20.56±0.0	18.46±0.0	13.56±0.0	12.55±0.0	9.56±0.05	8.56±0.42
	4	4	5	5	1		5
2	26.55±0.0	29.65±0.0	25.46±0.1	24.63±0.0	20.33±0.0	19.87±0.0	15.65±0.3
	5	5	46	3	5	1	47
3	38.79±0.0	38.46±0.0	34.56±0.3	36.87±0.0	32.46±0.0	21.59±0.3	23.49±0.3
	1	2	64	1	31	24	87
4	47.36±0.0	46.78±0.4	40.13±0.8	43.56±0.0	41.38±0.4	35.49±0.6	30.44±0.1
	5	51	7	6	15	31	4
5	54.65±0.0	53.25±0.0	49.65±0.1	54.68±0.0	49.50.056	43.99±0.9	39.76±0.4
	3	1	25	4	±	56	62

6	67.89±0.1	63.54±0.0	51.32±0.2	61.65±0.0	53.66±0.0	54.87±0.8	43.56±0.2
	36	2	36	3	3	43	5
7	76.56±0.0	72.46±0.0	60.15±0.1	78.36±0.0	69.78±0.0	61.47±0.1	51.36±0.1
	5	5	23	1	1	4	2
8	83.56±0.0	88.13±0.1	79.56±0.6	82.56±0.3	72.35±0.5	67.84±01	59.34±0.0
	6	36	54	64	4		5
9	89.46±0.0	84.56±0.1	87.65±0.3	88.46±0.3	79.88±0.1	70.16±0.2	67.23±0.6
	5	22	21	25	2		31
10	92.46±0.0	98.99±0.6	93±0.487	92±0.02	83±0.51	73±0.514	71±0.47
	1	87					

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Figure 24: Drug Release of L1-L13

#### Kinetic analysis of drug release-

In order to define the release mechanism that gives the best description of the release pattern; the in vitro release data for all optimized batches were fitted to kinetic equations models. The kinetic equations were used i.e., zero, first-order and Higuchi model. Both the kinetic rate constant (k) and the determination coefficient (R2) were calculated and presented in below graphs. The best fit model with the highest determination coefficient (R2) value for optimized batch was Zero order model.



Figure 25: Zero order model of L1-L13



 Table 37: Zero Order Model (L8)

Figure 26: First order model of L1-L13

 Table 38: First Order Model (L8)

First Order Model	
Formulation Code	R2 Value
L8	0.6074



Figure 27: Higuchi Model of L1-L13

#### Table 39: Higuchi Model (L8)

Higuchi Model					
Formulation Code	R2 Value				
L8	0.954				



Source	Sum Squares	df	Mean	F-	р-	
	of		Square	value	value	
Model	648.41	6	108.07	4.67	0.0413	significant
A-Sodium carboxymethyl	29.84	1	29.84	1.29	0.2993	
cellulose						
B-Sodium	97.37	1	97.37	4.21	0.0860	
glycolate						
starch						
C-glycerol	303.56	1	303.56	13.13	0.0110	
AB	30.25	1	30.25	1.31	0.2962	
AC	178.36	1	178.36	7.72	0.0321	
BC	9.03	1	9.03	0.3906	0.5550	
Residual	138.71	6	23.12			
Cor Total	787.12	12				

#### ANOVA for 2FI model Response 3: Drug release

#### **Final Equation in Terms of Actual Factors**

Drug release	=			
+274.99738				
-0.261069	Sodium carboxymethyl cellulose			
-14.18375	Sodium starch glycolate			
-101.56750	glycerol			
+0.013750	Sodium carboxymethyl cellulose * Sodium starch glycolate			
+0.133550	Sodium carboxymethyl cellulose * glycerol			
+6.01000	Sodium starch glycolate * glycerol			

The equation in terms of actual factors can be used to make predictions about the response for given levels of each factor. Here, the levels should be specified in the original units for each factor. This equation should not be used to determine the relative impact of each factor because the coefficients are scaled to accommodate the units of each factor and the intercept is not at the center of the design space.



Figure 28: Counter plot



Figure: 30 3D Surface plot

#### 7.2.12 Ex- vivo diffusion study

The ex-vivo diffusion study demonstrates that L8 is the optimized batch, showing superior performance among formulations L1-L13. L8 exhibits rapid initial drug permeation at 1 minute (19.63%  $\pm$  0.03), maintains high permeation at 5 minutes (54.18%  $\pm$  0.03), and achieves near- complete permeation at 10 minutes (97.89%  $\pm$  0.51).

			č	51			
Time	L1	L2	L3	L4	L5	L6	L7
(min)							
0	0	0	0	0	0	0	0
1	12.56±0	13.46±0.	15.60±0.	14.32±0.05	18.97±0.06	$14.56\pm00$	$14.35 \pm$
	.12	05	02	4		.03	0.06
2	24.53±0	38.79±0.	29.87±0.	26.54±0.03	28.46±0.01	23.55±0.	25.46±0
	.02	31	01	6		01	.02
3	39.87±0	39.74±0.	34.12±0.	38.78±0.74	37.40.056±0	32.45±0.	35.46±0

Table 40:	Drug	permeation	of	L1-	L7
		1			



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	.05	01	146	3	.453	06	.03
4	49.46±0	47.13±0.	45.66±0.	40.12±0.32	42.33±0.221	40.18±0.	45.56±0
	.06	02	036	4		01	.01
5	57.32±0	57.88±0.	56.49±0.	51.46±0.34	54.79±0.654	50.16±0.	53.65±0
	.01	03	045	7		05	.05
6	68.74±0	67.36±0.	68.47±0.	63.48±0.51	62.15±0.716	64.53±0.	66.49±0
	.05	354	01	113		01	.01
8	79.85±0	80.16±0.	78.46±0.	67.16±0.02	65.49±0.02	72.13±0.	73.56±0
	.06	345	02			05	.06
9	82.46±0	80.46±0.	86.45±0.	78.45±0.01	76.88±0.01	84.56±0.	86.65±0
	.05	06	04			06	.01
10	89.12±0	90.12±0.	89.71±0.	87.89±0.00	91.11±0.05	93.5 <u>6±</u> 0.	90.12±0
	.01	04	123	3		01	.01

All values expressed as mean ±STD

Table 41: Drug permeation of L8-L1.	Table 41:	Drug	permeation	of L8-L13
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			01			
Time	L8	L9	L10	L11	L12	L13
(min)						
0	0	0	0	0	0	0
1	19.63±0.03	15.32±0.01	13.46±0.18	12.01±0.01	11.87±0.87	14.56±0.06
2	38.79±0.01	26.53±0.35	20.46±0.97	21.35±0.02	18.96±0.364	21.56±0.07
3	38.79±0.04	37.89±0.14	37.46±0.87	34.55±0.79	29.56±0.254	30.16±0.05
4	49.78±0.14	43.56±0.34	48.32±0.78	49.97±0.87	37.13±0.387	40.13±0.03
5	54.18±0.03	53.14±0.65	58.94±0.65	52.36±0.54	46.25±0.964	51.36±0.54
6	65.87±0.05	65.44±0.33	69.88±0.34	67.46±0.94	53.44±0.03	61.45±0.63
8	75.59±0.04	78.93±0.62	77.65±0.34	$78.98 \pm 0.1$	64.31±0.04	72.36±0.74
9	87.89±0.01	86.54±0.87	89.13±0.12	80.16±0.02	75.66±0.05	81.13±0.34
10	97.89±0.51	94.56±0.961	91.23±0.47	88.87±0.01	80.13±0.03	89.56±0.01



Figure 31: % Drug Permeation of L1-L13

#### 7.2.13 Stability study

The stability studies of the L8 optimized batch indicate excellent stability over a 90-day period. The

drug content remains consistent at 96.48% throughout the study, demonstrating that the active ingredient's concentration does not degrade over time.

Sr.no	Time in days	Drug Content (%)	Disintegration time	In –vitro drug release
			(sec)	(%)
1.	Initial (0 days)	96.48	22	98.99
2.	1 month (30 days)	96.48	22	98.99
3.	3 months(90days)	96.48	21	98.78

 Table 41: Stability studies data of L8 optimized batch

#### CONCLUSION

The formulation study of Lisinopril tablets identified Batch L8 as the most promising candidate due to its superior physical and chemical properties. It displayed consistent weight, ideal pH, appropriate viscosity, high drug content, and an excellent in vitro release profile, with 98.67% of the drug released over 12 hours. The stability of Batch L8 was confirmed through zeta potential measurements and long-term stability testing, making it a suitable candidate for further development and potential clinical application

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